# Validity of ECSC prediction equations for spirometric indices in Dutch conscripts

W.H. Stevens\*, J.H. van Hartevelt\*\*, P.E.K. The\*, H.A.J. Smink\*, Ph.H Quanjer\*\*

Validity of ECSC prediction equations for spirometric indices in Dutch conscripts. W.H. Stevens, J.H. van Hartevelt, P.E.K. The, H.A.J. Smink, Ph.H Quanjer. ©ERS Journals Ltd 1994.

ABSTRACT: A study was performed to determine whether prediction equations issued by the European Community for Steel and Coal (ECSC) and the European Respiratory Society (ERS) fit spirometric data in young adult males. The study comprised 246 randomly selected Dutch conscripts, who participated in the study on the basis of informed consent.

A questionnaire was used to assess respiratory symptoms and smoking habits. Maximal expiratory flow-volume curves were obtained with a rolling seal spirometer, and summary statistics selected according to ECSC/ERS recommendations. In addition, standing height and body weight were obtained.

We analysed the data of 100 conscripts of European descent, with no history of respiratory symptoms. They were all life-long nonsmokers. Their mean (sD) age was 18 (0.12) yrs (range 17.9–19.0 yrs), with a mean (sD) standing height of 1.84 (0.06) m (range 1.68–2.00 m). The data for forced vital capacity (FVC), forced expiratory volume in one second (FEV<sub>1</sub>) and maximal mid-expiratory flow (MMEF) agreed well with ECSC predictions; 95% confidence intervals (95% CI) of differences between measured and predicted values were -0.174 to 0.044 *l*, -0.012 to 0.174 *l*·s<sup>-1</sup> and -0.114 to 0.302 *l*·s<sup>-1</sup>, respectively. Peak expiratory flow was systematically larger than predicted, as was FEV<sub>1</sub>%FVC (95% CI 0.74 to 1.31 *l*·s<sup>-1</sup> and 2.50 to 5.24%, respectively), due to the intercept being inappropriate. The residual standard deviation in the conscripts was somewhat less than in the ECSC/ERS predictions equations, except for peak expiratory flow (PEF). The percentages of observations below the predicted lower limit were 9% for FVC, 5% for FEV<sub>1</sub>, 2% for FEV<sub>1</sub>%FVC, 2% for PEF, and 4% for MMEF.

We conclude that the ECSC/ERS recommendations are satisfactory for  $FEV_1$ , FVC and MMEF. However,  $FEV_1\%$  FVC and PEF are systematically higher than predicted, but this does not preclude the use of prediction equations for diagnostic and discriminatory purposes.

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Lung volumes and forced ventilatory flows are routinely assessed in patients with suspected obstructive lung disease. In particular, forced expiratory volume in one second (FEV<sub>1</sub>), forced vital capacity (FVC), peak expiratory flow (PEF) and forced expiratory flow during the middle half of the FVC (MMEF) are often used for that purpose. Some laboratories also use the maximal expiratory flow at 75, 50 or 25% of the FVC (MEF<sub>75</sub>, MEF<sub>50</sub> and MEF<sub>25</sub>, respectively) in lung function assessment. Reference values for the 18–20 year age range are scarce, since this age group tends to be excluded in studies both on adolescents and adults. In 1983, a working party of The European Community for Steel and Coal (ECSC) issued recommendations on reference values for ventilatory indices [1], and suggested that between the ages 18-25 yrs cross-sectionally there is no change in ventilatory function, so that an age of 25 yrs can be used in the regression equations. Recently the ECSC and European Respiratory Society (ERS) updated the recommendations,

\*Dept of Medical Affairs for Conscripts, Ministry of Defense, The Netherlands. \*\*Physiology Dept, Leiden University, Leiden, The Netherlands.

Correspondence: Ph.H. Quanjer Physiology Dept P.O. Box 9604 2300 RC Leiden The Netherlands

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but those for reference values were unaltered [2]. However, there is evidence which suggests that lung volumes and forced ventilatory flows in males increase up to 25–30 yrs [3–10], so that the validity of this recommendation can be questioned.

The present study was designed to assess the validity of the ECSC recommendations on reference values in young male adults. Subjects included in this study were conscripts, who had received a call up for the mandatory medical examination at age 18 yrs. They were studied at one of the examination centres of the Armed Forces.

## Methods

Subjects

As only males are conscripted into the army, all subjects participating in the study were males. The participants

were randomly selected upon reporting at the desk at the medical examination centre for conscripts in Amsterdam. Each person participated voluntarily in the tests of ventilatory function, after being informed of the objectives. Spirometric tests were performed on the day of their medical testing in the period April–July 1991, on working days between 9 am and 4 pm.

Subjects were included in the study if they met the following criteria: 1) lifetime nonsmoker; 2) no symptoms of lung, heart or chest disease in the past of present; 3) of European descent; 4) having Dutch nationality; and 5) producing at least three technically satisfactory maximum expiratory flow-volume (MEFV) curves. The study was approved by the Medical Ethics Committees of the Armed Forces and the Academic Hospital of Leiden University.

#### Data collection

Each of the subjects filled out a self-administered Medical Research Council (MRC)-ECSC questionnaire [11], which formed the basis for assessing the respiratory health status. Standing height was measured to the nearest mm without shoes, and weight was measured (in kg) without shoes and with light indoor clothing

Spirometry was performed with a Mijnhardt rolling seal spirometer (Vicatest type 5) fitted with a pulse encoder, which replaced the standard potentiometer. The encoder produces a pulse of 5 V when the volume changes by 20 ml. A second pulse from the pulse encoder, which was out of phase with the first, was used to discriminate between inspiration and expiration. Sampling was initiated by the start of the forced expiratory manoeuvre, and terminated when there had been no volume change in 0.3 s. The spirometer was connected to a computer via a LabMaster Data Acquisition System (Scientific Solutions). The time between two pulses of the pulse-encoder was determined with a resolution of 10 ms. The flow was obtained by differentiating the volume change with respect to time. A thermometer with digital display was fitted into the spirometer, so that its interior temperature could be read during measurements.

Prior to the study, the equipment had been validated; the spirometer had a frequency-response flat to 20 Hz sufficiently high to comply with ECSC [1, 2] and American Thoracic Society (ATS) [12] recommendations. The equipment was calibrated weekly by means of a 3 *l* calibrated syringe; the readings were stable, and therefore no parameter was changed during the study.

Prior to spirometric measurements, the procedure was explained and demonstrated to each subject. In the case of faulty manoeuvres, the display of the flow-volume loop was helpful in explaining how to improve the performance. All measurements were performed on seated subjects, sitting upright, and fitted with a noseclip. A minimum of three and a maximum of five technically acceptable flow-volume curves was obtained in each subject. From each set of flow-volume curves, a composite MEFV-curve was generated by the computer. This curve comprised the largest values for FVC and PEF, and the largest values of flows derived from curves with an FVC within 5% of the largest FVC, according to recommendations

[1, 2]. The MMEF is similarly the largest value from an FVC within 5% of the largest FVC, and the FEV<sub>1</sub> the largest value recorded.

All volumes and flows have been corrected to body temperature and pressure, saturated (BTPS) conditions.

#### Data analysis

Since all subjects were less than 25 yrs old, predicted values were obtained by substituting 25 yrs in the prediction equations, in keeping with ECSC recommendations [1, 2]. We then computed the difference between measured and predicted values for each index. The distribution of these residuals was then studied, i.e. their mean and standard deviation. In the case of a good fit to the ECSC predictions, the mean comes to nil, and the standard deviation is equal to the residual standard deviations (RSD) quoted in the ECSC report [1, 2]. In keeping with the ECSC recommendation, the lower 5th percentile was computed by subtracting 1.64×RSD from the predicted value; this value was then compared to the 5th percentile actually observed in this population, and the percentage of subjects that fell below the ECSC 5th percentile. In addition, spirometric indices were regressed on standing height, as well as on standing height and body mass index (BMI). BMI is conventionally taken to be body weight (W) divided by height (H) squared; however, in previous work on adolescents, we had observed that BMI still correlated with standing height. In order to remove any correlation between height and BMI, we therefore computed the best fit between log(weight) and log(height) of the form  $log(W)=a+k\times log(H)$ , and used BMI=W/H<sup>k</sup> in further analyses. Since the standard deviation of age came to only 0.12 yrs, age was not used in any of the computations. Statistical analysis was performed with the Number Cruncher Statistical System (NCSS) package [13].

## Results

A total of 294 subjects was selected to take part in the study. Two persons refused to participate; six persons, who had agreed to participate, could not be tested because the time schedule for the medical examination was not compatible with that of the spirometric measurements. The data of 17 subjects could not be used, because they did not produce three acceptable forced vital capacity manoeuvres. One hundred subjects met the requirement that they never had respiratory symptoms, had been lifetime nonsmokers, were of Caucasian extraction, and had Dutch nationality (reference group). The remaining 169 subjects did not meet these criteria. The subjects lived both in urban and rural environments.

The mean age (sD) of the 100 reference subjects was 18.0~(0.12) yrs (range  $17.9{\text -}19.0$  yrs), the mean height 1.84~(0.06) m (range  $(1.676{\text -}1.995$  m), and the mean body mass 73.1~(9.2) kg (range  $50{\text -}98$  kg). The relationship between body mass in kg (W) and standing height in m (H) was: W= $24.16{\times}\text{H}^{1.81}$  (r=0.4891). For each individual, the BMI was therefore obtained as W/H<sup>1.81</sup>; the mean (sD) was 24.30~(2.73), and the range  $18.57{\text -}34.25$ .

Table 1. - Regression models of relationship between spirometric indices and anthropometric variables

	Regression coefficients				
Index	Intercept	Height	BMI	RSD	r
FVC l	-6.273	+5.677	+0.056	0.534	0.5915
$FEV_1 l$	-4.701	+4.543	+0.046	0.459	0.5660
PEF $l \cdot s^{-1}$	-3.283	+5.676	+0.174	1.393	0.3945
MMEF l·s-1	-2.811	+3.577	+0.063*	1.040	0.2640
$\text{MEF}_{75} l \cdot s^{-1}$	+2.487	+1.620**	+0.136	1.470	0.2546
$\text{MEF}_{50} l \cdot s^{-1}$	-3.260	+4.093*	+0.089*	1.334	0.2579
$MEF_{25}^{56} l \cdot s^{-1}$	-4.254	+3.858	+0.020**	0.879	0.2750
	Regression coefficients				
Index	Intercept	ln(Height)	BMI	RSD	r

	Regression coefficients				
Index	Intercept	ln(Height)	BMI	RSD	r
ln(FVC)	-0.417	+1.951	+0.293	0.1016	0.5944
$ln(FEV_1)$	-0.431	+1.856	+0.270	0.1001	0.5784
ln(PEF)	+0.622	+0.962	+0.382	0.1249	0.3979
ln(MMEF)	-0.152	+1.317	+0.312*	0.2099	0.2640
$ln(MEF_{75})$	+0.645	+0.435**	+0.391	0.1784	0.2508
$ln(MEF_{50})$	-0.034	+1.236*	+0.351	0.2252	0.2498
$ln(MEF_{25})$	-0.633	+2.181	+0.147**	0.2752	0.2704

<sup>\*: 0.10&</sup>gt;p>0.05; \*\* p>0.10. BMI: W/H<sup>1.81</sup>, where W=weight in kg and H=stature in metre; RSD: residual standard deviation; r: correlation coefficient; FVC: forced vital capacity; FEV<sub>1</sub>: forced expiratory flow volume in one second; PEF: peak expiratory flow; MMEF: maximal mid-expiratory flow; MEF<sub>75</sub>, MEF<sub>50</sub> and MEF<sub>25</sub>: maximal expiratory flow at 75%, 50% and 25% of FVC, respectively.

The following models were tested:

$$Y=a_1+b_1\times H+c_1\times BMI \tag{1}$$

$$lnY = a_2 + b_2 \times lnH + c_2 \times BMI$$
 (2)

$$lnY = a_3 + b_3 \times H + c_3 \times BMI$$
 (3)

where Y=lung function index. The results obtained with the different models are given in table 1. The explained variance and the fit to model (2) was nearly identical to that of model (3); hence, results with the latter approach are not included in the table. FEV<sub>1</sub>%FVC was not correlated to either height, age or BMI. PEF, MMEF, MEF<sub>75</sub>, MEF<sub>50</sub> and MEF<sub>25</sub> correlated poorly with standing height: the explained variance was between 6 and 16% (table 1).

Table 2. – Comparison of regression coefficient of ventilatory function on standing height (95% confidence interval) in the present study and that in prediction equations [1, 2]

Index	95% CI	ECSC	
FVC	3.89-7.39	5.76	
$FEV_1$	3.02-6.01	4.30	
MMEF	0.23 - 6.84	1.94	
PEF	0.94-8.70	6.14	
MEF <sub>75</sub>	-3.23-6.30	5.46	
MEF <sub>50</sub>	-0.03-8.30	3.79	
MEF <sub>25</sub>	1.08-6.61	2.61	

95% CI: 95% confidence interval; ECSC: European Community for Steel and Coal. For further abbreviations see legend to table 1

Table 3. – Difference between observed and predicted values for ventilatory indices, and comparison of residual standard deviation (RSD) in present study and in ECSC/ERS document [1, 2]

Index	Mean	95%CI	RSD	
			Conscripts	ECSC
FVC l	-0.07	-0.17-0.04	0.55	0.61
$FEV_1$ $l$	+0.08	-0.01-0.17	0.47	0.51
FEV <sub>1</sub> %FVC %	+3.87	+2.50-5.24	6.91	7.17
PEF $l \cdot s^{-1}$	+1.02	+0.74-1.31	1.46	1.21
MMEF $l \cdot s^{-1}$	+0.09	-0.11-0.30	1.04	1.04
$\text{MEF}_{75} l \cdot s^{-1}$	-0.06	-0.37-0.23	1.52	1.71
$\text{MEF}_{50} l \cdot s^{-1}$	+0.59	+0.32-0.85	1.34	1.32
$\text{MEF}_{25} \ l \cdot s^{-1}$	+0.51	+0.33-0.68	0.88	0.78

ERS: European Respiratory Society. For further abbreviations see legends to table 1 and 2.

The regression coefficients for standing height were not significantly different from those in the ECSC document (table 2). In keeping with this, the difference between actual and predicted value was not related to standing height for any of the flow-volume indices (0.1053 <p<0.9086).

Table 3 summarizes the difference between measured and predicted values. The standard deviations about the mean were similar to those in the ECSC recommendations, which were generally somewhat larger. There were no systematic differences between measured and predicted FVC, FEV<sub>1</sub>, and MMEF, but observed values for PEF and FEV<sub>1</sub>%FVC were systematically higher than those predicted by the ECSC (table 3).

The specificity of tests, *i.e.* the proportion of subjects correctly identified as forming part of the reference population, is influenced by the distribution of test results. The lower 5th percentiles according to the ECSC document, the actual 5th percentile observed in the 100 subjects, and the number of subjects in whom measured values fell below the lower limit recommended by the ECSC are shown in table 4. The specificity varied between 91% (FVC) and 99% (MEF $_{25}$ ) (table 4).

Table 4. – Comparison of lower 5th percentiles (actual - predicted value) according to ECSC/ERS document and that observed in the 100 conscripts, and the percentage of subjects falling below the lower ECSC/ERS limit

Index	Actual percentile	Predicted lower limit	% subjects
FVC l	-1.333	-1.000	9
$FEV_1 l$	-0.859	-0.839	5
FEV <sub>1</sub> %FVC %	-9.53	-11.79	2
PEF $l \cdot s^{-1}$	-1.57	-1.99	2
MMEF $l \cdot s^{-1}$	-1.666	-1.710	4
$MEF_{75}$ $l \cdot s^{-1}$	-2.500	-2.812	4
MEF <sub>50</sub> <i>l</i> ·s <sup>-1</sup>	-1.648	-2.171	3
$MEF_{25} l \cdot s^{-1}$	-0.811	-1.283	1

For abbreviations see legends to tables 1–3.

#### Discussion

In the Netherlands, all boys are, in principle, eligible to be conscripted into the army. Hence, each of them is medically examined. Therefore, the subjects participating in this study form an unselected sample of the population of conscripts. In these naive subjects, we generally found satisfactory agreement between the predicted and observed values for most spirometric indices. Whilst the age coefficient could not be tested, the regression coefficient of ventilatory function on standing height in the ECSC document appears to be compatible with that in this population of young adults. The most commonly used indices, i.e. FEV<sub>1</sub> and FVC, agree remarkably well with the predicted values, so that these predictions appear to be quite valid for screening purposes and for clinical use. However, the intercept for PEF is about 1  $l \cdot s^{-1}$  too low in the ECSC prediction equations, and FEV<sub>1</sub>%FVC about 3.9% too low (table 3). On that account, 2% rather than 5% of subjects have a value for PEF and FEV<sub>1</sub>%FVC below the recommended lower limit of normal. For FVC this comes to 9%; this is due to a group of subjects who seem to form a population distinct for the other reference subjects (fig. 1).

The fair overall agreement between ECSC predictions and the observed values, whilst satisfactory and reassuring, may not hold true for populations elsewhere in Europe. The ECSC equations derived from a mix of historic data, which showed considerable discrepancies [1]; the original material had been collected up to three decades ago, when the selection of subjects, equipment, measurement techniques, procedures adopted, etc. must have been different from that in the present study. In addition, cohort effects [14], and the changing relationship between trunk and total height [15] of successive birth cohorts, might have led to a changing relationship between standing height and ventilatory function. On the other hand, MERKUS and QUANJER [16] found no evidence of a time-related trend in prediction equations for children and adolescents [16].

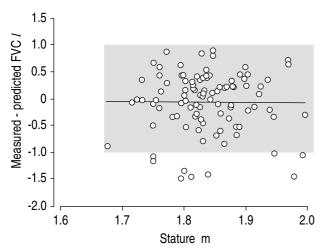


Fig. 1. – Relationship between measured and predicted FVC [1, 2], plotted as a function of stature. Solid line is the regression line of actual minus predicted FVC on stature. The boxed area delineates the 5th and 95th percentile according to [1, 2]. FVC: forced vital capacity.

In general, the variance explained by height is low, and less than that reported in adults in the literature. This is probably, in part, due to the small range in height in the present study. In the age range 20–70 yrs there is a greater scatter in standing height, due to older generations being systematically smaller than young adults. In the present population the range in standing height is 32 cm, whilst in a previous study of Dutch males aged 20–70 yrs the range was 44 cm [1]. Non-linear relationships between the ventilatory index and independent variables (models (2) and (3)) have no advantage over simple, linear models (table 1), a conclusion reached previously by DROUET *et al.* [17].

The body mass index contributed significantly to reducing the variance of spirometric indices, except for effort independent flows. This finding cannot be interpreted unequivocally: a high value for this index may be due to increased body fat, or greater muscularity; a low one may be associated with a very slender body build or long legs for height [18]. Hence, it is not clear whether the contribution of the BMI primarily reflects variability in muscularity; the positive correlation of BMI to effort dependent indices of ventilatory function suggests that a more athletic body build and greater muscle force are the most plausible explanations. A more direct measure of the contribution of respiratory muscle strength can be derived from measurement of maximal inspiratory and expiratory pressure, at different lung volumes. Thus, LEECH et al. [19], GAULTIER and ZINMAN [20], and SCHRADER et al. [21] showed that muscularity does contribute, somewhat, to explaining differences in ventilatory function between subjects.

FEV, %FVC was systematically higher in conscripts than predicted, so that only 2% of the values fell below the predicted lower limit of normal; this may have bearing in clinical practice and in screening, as the index is often used. If the prediction is too low, then the specificity of the test increases, i.e. a greater proportion of healthy subjects is correctly identified. On the other hand, the sensitivity, *i.e.* the proportion of patients with airflow limitation correctly identified, diminishes likewise. The decrease in the proportion of false positive test results is, therefore, associated with an increase in the proportion of false negative test results. In fact, the recommendation to substitute 25 yrs in the prediction equation for people younger than 25 yrs may not be logical. This is because, in many studies, the FEV<sub>1</sub>/FVC ratio has been found to decrease steadily in adolescents, even though FEV, and FVC increase due to growth (overview in [22]). It is therefore likely that this decrease continues up to age 25 yrs, and beyond. If, on that account, the actual age is substituted in the prediction equation, the lower limit of normal in the conscripts changes to -10.79% below the predicted mean FEV<sub>1</sub>%FVC (fairly close to that predicted by the ECSC) (table 4), and 3% have values below the lower limit of the ECSC; this represents only a small change in this material. We suggested that, in practice, reliance should be placed primarily on the FEV, and FVC, and the ratio be considered only secondarily, adopting a 5th percentile which is 10% below the predicted FEV<sub>1</sub>%FVC. However, further studies are required

to show that our findings also apply to other populations, before undue reliance is placed on the results of the present study.

The recorded peak expiratory flow was systematically higher than predicted. This might, in principle, be due to the rolling seal spirometer being unsuitable for measurements of PEF. However, the frequency response of the instrument has been shown to be sufficient for measurements of PEF [23-25]. It is more likely that the ECSC predictions for PEF are too low when applied to pneumotachometers and spirometers with a fast rise time, since the peak flow meter underestimates PEF if it is reached in less than 100 ms [26]. We found, in a separate study, that 50% of adolescents reach PEF in less than 100 ms (unpublished observations). The ECSC summary equations derive from a mix of pneumotachometer and peak flow meter recordings, and may, therefore, give values which are too low for low resistance instruments with a good dynamic response. In the updated standardization report, the ECSC and ERS recommend that more work is needed to establish acceptable reference equations for PEF, and our findings tend to support that view.

In general, flows towards the end of the forced vital capacity manoeuvre are greater than predicted (table 3). This reflects MEFV-curves which are more convex towards the volume axis than predicted in adults. This is compatible with increased stiffness of the thoracic cage during growth, so that residual volume in young adults is primarily determined by the elastic properties of the thorax; whilst in older subjects the elastic properties of the lung are a more important determinant [27]. Flows at specified percentages of the FVC are poorly predictable (table 1) (review in [1]); in addition, they are dependent on the FVC, which is itself influenced by both lung disease and extrapulmonary factors. This implies that these indices should not be used for screening purposes. Hence, we suggest that there is no purpose in supplying prediction equations for these indices, or in using them for screening purposes.

In conclusion, these data suggest that the ECSC summary equations for FEV<sub>1</sub>, FVC and MMEF are applicable in 18 year old healthy males, both for screening purposes and clinical work. The FEV<sub>1</sub>/FVC ratio in young subjects is systematically greater than predicted, but there are reasons to suggest that the actual age, rather than 25 yrs, should be substituted in the prediction equations. Flows towards the end of the forced vital capacity manoeuvre are systematically higher than predicted in young adults, but the usefulness of these indices is doubtful anyway, and, therefore, this finding is of little consequence.

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### References

Quanjer PhH (ed). – Standardized lung function testing. Report Working Party "Standardization of Lung Function Tests", European Community for Steel and Coal.

- 2. Quanjer PhH, Tammeling GJ, Cotes JE, Pedersen OF, Peslin R, Yernault J-C. Lung volumes and forced ventilatory flows. Report Working Party "Standardization of
  - tilatory flows. Report Working Party "Standardization of Lung Function Tests", ECSC, Official Statement European Respiratory Society. *Eur Respir J* 1993; 6 (Suppl. 16): 5–40.

Bull Eur Physiopathol Respir 1983; 19 (Suppl. 5): 1–95.

- 3. Schoenberg JB, Beck GJ, Bouhuys A. Growth and decay of pulmonary function in healthy blacks and whites. *Respir Physiol* 1978; 33: 367–393.
- 4. Hurwitz S, Allen J, Liben A, Becklake M. Lung function in young adults: evidence for differences in the chronological ages at which various functions start to decline. *Thorax* 1980; 35: 615–619.
- Burrows B, Cline MG, Knudson RJ, Taussig LM, Lebowitz MD. A descriptive analysis of the growth and decline of the FVC and FEV<sub>1</sub>. *Chest* 1983; 83: 717–724.
- Dockery DW, Ware JH, Ferris BG, et al. Distribution of forced expiratory volume in one second and forced vital capacity in healthy, white, adult never-smokers in six US cities. Am Rev Respir Dis 1985; 131: 511–520.
- Burrows B, Lebowitz MD, Camilli AE, Knudson RJ. Longitudinal changes in forced expiratory volume in one second in adults. Methodological considerations and findings in healthy nonsmokers. *Am Rev Respir Dis* 1986; 133: 974–980.
- 8. Tager IB, Segal MR, Speizer FE, Weiss ST. The natural history of forced expiratory volumes. *Am Rev Respir Dis* 1988; 138: 837–847.
- 9. Sherrill DL, Camilli A, Lebowitz MD. On the temporal relationship between lung function and somatic growth. *Am Rev Respir Dis* 1989; 140: 638–644.
- Kristufek P, Brezina M, Ciutti P, Strmen J, Mayer M. Reference values and modelling of lung function development as a transcendent function of age, body height and mass. *Bull Eur Pathophysiol Respir* 1987; 23: 139–147
- 11. Van der Lende R, Orie NGM. The MRC-ECSC questionnaire on respiratory symptoms. Use in epidemiology. *Scand J Respir Dis* 1972; 53: 218–226.
- 12. ATS Statement. Standardization of spirometry 1987 update. *Am Rev Respir Dis* 1987; 136: 1285–1289.
- Number Cruncher Statistical System. JL Hintze, Kaysville, Utah, 1991.
- Glindmeyer HW. Predictable confusion. J Occup Med 1981; 23: 845–849.
- Tanner JM, Hayashi T, Preece M, Cameron N. Increase in length of leg relative to trunk in Japanese children and adults from 1957 to 1977: a comparison with British and with Japanese Americans. *Ann Hum Biol* 1982; 9: 411– 423.
- Merkus PJFM, Quanjer PhH. Cohort effects and paediatric pulmonary reference values. Eur Respir J 1990;
  3: 299s.
- Drouet D, Kauffman F, Brille D, Lellouch J. Valeurs spirographiques de référence. Modèles mathématiques et utilisation pratique. *Bull Eur Physiopathol Respir* 1980; 16: 747–767.
- Garn SM, Leonard WM, Hawthorne VM. Three limitations of the body mass index. Am J Clin Nutr 1986; 44: 996–997.
- Leech JA, Ghezzo H, Stevens D, Becklake MR. Respiratory pressures and function in young adults. Am Rev Respir Dis 1983; 128: 17–23.
- Gaultier C, Zinman R. Maximal static pressures in healthy children. Respir Physiol 1983; 21: 45–61.
- 21. Schrader PC, Quanjer PhH, Olievier ICW. Respiratory

- muscle force and ventilatory function in adolescents.  $Eur\ Respir\ J\ 1988;\ 1:\ 368-375.$
- Quanjer PhH, Stocks J, Polgar G, Wise M, Karlberg J, Borsboom G. Compilation of reference values for lung function measurements in children. *In*: Quanjer PhH, Helms P, Bjure J, Gaultier C, eds. Standardization of lung function tests in paediatrics *Eur Respir J* 1989; 2 (Suppl. 4): 184s–261s.
- 23. Peslin R. Frequency response of pneumotachographs. *Bull Physiopathol Respir* 1972; 8: 1363–1376.
- Kruyt EW, Van Hartevelt JH, Quanjer PhH, Douma JH.
  Frequency requirements for pneumotachometers for

- recording maximum expiratory flow-volume curves. *Bull Eur Physiopathol Respir* 1982; 18: 42p–43p.
- Peslin R, Jardin P. Influence of second-order data filtering on common forced expiration indices. *Clin Physiology* 1983; 3: 123–130.
- Miller M, Pedersen OF. The characteristics and calibration of devices for recording peak expiratory flow. International workshop on peak expiratory flow. Brussels, September 1991.
- Leith DE, Mead J. Mechanisms determining residual volume of the lungs in normal subjects. *J Appl Physiol* 1967; 23: 221–227.