Automatic regulation of the cuff pressure in endotracheallyintubated patients

R. Farré*, M. Rotger*, M. Ferrer*, A. Torres*, D. Navajas*

Automatic regulation of the cuff pressure in endotracheally-intubated patients. R. Farré, M. Rotger, M. Ferrer, A. Torres, D. Navajas. ©ERS Journals Ltd 2002. ABSTRACT: To avoid tracheal wall damage or inadvertent falls of the endotracheal tube cuff pressure (Pcuff) in intubated and mechanically-ventilated patients, the authors devised a simple procedure for automatic and continuous regulation of Pcuff.

The procedure, only requiring a simple aquarium air pump and conventional tubing, was first tested at the bench when applied to an intubated and ventilated lung model, including an artificial trachea with an externally-variable section. The clinical performance of the procedure was tested in eight intubated patients, in whom the endotracheal tube cuff was connected to the designed *Pcuff* regulator during 24 h.

The bench test showed that the procedure was able to maintain $P_{\rm cuff}$ constant, regardless of the changes imposed in the tracheal section. It was also effective in maintaining $P_{\rm cuff}$ during routine mechanical ventilation. Actual $P_{\rm cuff}$ recorded over the 24-h period always coincided with the target value within ± 2 cmH₂O in all the patients.

The procedure devised to maintain endotracheal tube cuff pressure is readily implemented, cheap, easy to operate and can be used regardless of the specific ventilator or tube used. Routine implementation of this procedure may be useful for protecting the trachea from tissue damage and for reducing the risk of ventilator-associated pneumonia.

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Ventilator-associated pneumonia (VAP) is the most relevant complication in mechanically-ventilated patients, given its high incidence, associated morbidity and mortality, and economic cost [1-3]. The most important pathogenic mechanism of VAP is the aspiration to the lower airways of contaminated secretions pooled above the endotracheal tube cuff [4]. Maintaining adequate inflation pressure of the endotracheal tube cuff (Pcuff) is a key factor in the management of the patient/ventilator interface during invasive mechanical ventilation [5-7]. An excessively inflated cuff reaching Pcuff levels above the mucosal capillary pressure [8], although not frequent when using endotracheal tubes with a high-volume lowpressure cuff, has recently been reported to cause ischaemic tracheal wall injury [9]. Moreover, loss of cuff inflation is a much more frequent complication [10, 11]. Persistently low Pcuff has been identified as a risk factor for VAP [11]. Consequently, ensuring a correct inflation of the endotracheal tube cuff has been recommended [4].

Routine management of Pcuff in intubated patients is generally performed by manually checking with a

periodicity of several hours, which does not ensure adequate P_{cuff} maintenance during continuous endotracheal intubation [11]. Furthermore, manual checking of P_{cuff} may result in the aspiration to the lower airways of contaminated secretions pooled above the cuff. To avoid these problems, the authors devised and tested a simple procedure for automatically and continuously ensuring adequate P_{cuff} in the intensive care unit (ICU) environment.

Methods

The present authors devised a simple procedure for continuously and automatically regulating $P_{\rm cuff}$ in mechanically-ventilated patients (fig. 1). This system shares the same principle of continuous positive airway pressure devices, since the pressure applied to the cuff is generated by the passage of an airflow through a resistor. A small (8×4×4 cm³), low cost (<12 Euros) aquarium air pump (Nathura MK-701, 2.5 W; ECIS, Bressanvido, Italy) generated a pulsating flow with an amplitude determined by a simple

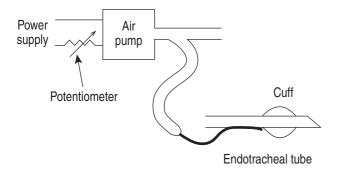


Fig. 1.–Diagram of the cuff pressure regulation system. A domestic aquarium air pump is connected to the main power supply (110/220 V). The voltage provided to the pump is determined by means of a resistive potentiometer. The air outlet of the pump is connected to a leak tube (9 cm in length, 1 mm in diameter) open to the atmosphere and to a flexible tube (2 m in length, 2 mm diameter), allowing the pump be placed at a convenient distance from the endotracheally-intubated patient.

potentiometer (20 k Ω , 5 W). The outlet of the pump was connected to a tube 9 cm in length and 1 mm in diameter, which was open to the atmosphere. The endotracheal tube cuff was connected to the pump by means of a flexible tubing 2 m in length and 2 mm in diameter (conventional pressure extension line for arterial catheter), allowing the pump to be placed at a convenient distance from the patient. This tube was ended with conventional connectors to maintain a permanently open cuff valve. The tubing and the cuff connected to the pump acted as a pneumatic low-pass filter that converted the oscillating pump flow into a constant pressure ($\pm 0.2 \text{ cmH}_2\text{O}$) inside the cuff. The potentiometer, which was calibrated in terms of pressure for this specific pump and tubing, allowed setting the Pcuff to 15–45 cm \hat{H}_2O .

The procedure was first tested at the bench to assess whether it was possible to keep a constant Pcuff under demanding conditions. An 8-mm endotracheal tube (Hi-Lo, Mallinckrodt Medical, Athlone, Ireland) was used to intubate and ventilate (20 breath min⁻¹, 0.5 L tidal volume; Servo ventilator 900C, Siemens, Solna, Sweden) a resistance-compliance lung model (Test Lung 190, Siemens) connected through an artificial trachea (nonrigid polyvinyl chloride (PVC) tube of 15 cm in length and 2.5 cm in internal diameter) [12]. Pressure at the outlet of the Pcuff regulator was recorded (30 Hz low-pass filter; MP-45, Validyne, Northridge, CA, USA), while tracheal section at the level of the endotracheal cuff was modified by means of an actuator applied to the external wall of the artificial trachea.

The clinical feasibility of the Pcuff regulation procedure was assessed in eight sedated, intubated and mechanically-ventilated patients for ≥ 24 h before starting the study and they were consecutively admitted to the Respiratory ICU because of respiratory failure. The Ethical Committee of the Hospital approved the protocol and informed consent was obtained from patients' next-of-kin in all cases. In two of these patients, the valve built into the cuff tubing developed a considerable air leak (time constants of 3 and 10 min). In these two patients, maintaining

cuff inflation had required additional clamping of the cuff valve and frequent controls by the attending nurses. In each patient, the *P*cuff regulator was applied for a period of 24 h and *P*cuff was continuously measured (174PC28HD2, Honeywell, Freeport, IL, USA). The pressure signal was sampled, digitally filtered to eliminate the oscillations due to ventilator cycling, and stored on a computer.

Results

The bench test showed that the devised pressure regulation procedure was able to maintain Pcuff regardless of the changes imposed in the tracheal diameter. Figure 2a shows the time course of the Pcuff during baseline mechanical ventilation (0–12 s) and after a sudden decrease (12–43 s) and increase (43–60 s) in tracheal area in the conventional setting (i.e. when the cuff was inflated and kept closed by its own valve). As expected, Pcuff underwent a considerable increase/decrease (to 70 and 2 cm H_2O during expiration, respectively, from the baseline of 30 cm H_2O) as a result of a reduction/increase in tracheal area. The periodic changes (20 cycles·min⁻¹) observed

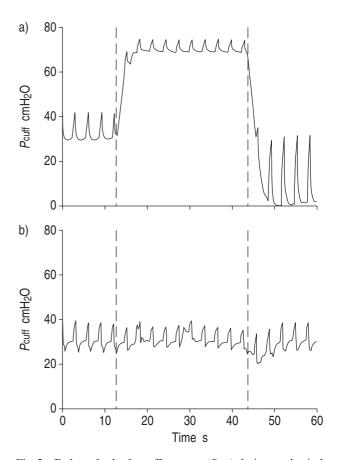


Fig. 2.—Endotracheal tube cuff pressure (*P*cuff) during mechanical ventilation of a respiratory system model, including a trachea with externally-controlled section. Time 0–12 s: baseline tracheal section; time 12–43 s: decreased tracheal section; time 43–60 s: increased tracheal section. a) Conventionally inflated cuff; b) application of the devised procedure to maintain cuff pressure.

1012 R. FARRÉ ET AL.

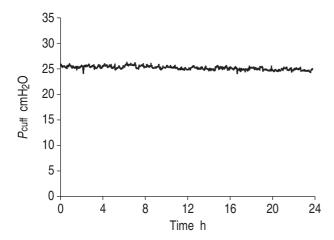


Fig. 3.—Example of the endotracheal tube cuff pressure (P_{cuff}) during a 24-h period of mechanical ventilation in a patient. P_{cuff} was digitally filtered to eliminate the tidal oscillations due to the ventilator cycling.

in *P*cuff were induced by the change in tracheal pressure due to the ventilator cycling [13, 14]. By contrast, when the designed regulation system was used (fig. 2b), *P*cuff remained constant as the artificial trachea was subjected to the same challenge.

The results obtained in the study of routine patients confirmed that the procedure devised was effective in regulating $P_{\rm cuff}$ in all the patients. Figure 3 shows the 24-h recording of $P_{\rm cuff}$ in the patient whose cuff valve developed the greatest leak (i.e. the most demanding case in terms of keeping constant cuff inflation). Actual $P_{\rm cuff}$ was maintained at the target value within $\pm 2~{\rm cmH_2O}$ over the 24-h period in all the patients. The attending staff reported no particular incident with regard to $P_{\rm cuff}$.

Discussion

The procedure that has been described and tested was effective in maintaining Pcuff during routine mechanical ventilation. As shown in figure 2, the system exhibited a fast response under challenging conditions that would represent extreme changes in Pcuff in the clinical setting. The changes in cuff compression imposed in the bench study covered the ones that can reasonably be found in patients as a result of displacement of the endotracheal tube, a change in the tracheal wall tone, diffusion of anaesthetic gases [15] or hypothermic surgical procedures [16]. In particular, the fast response time of the devised procedure ensures its efficacy in compensating for leaks in the cuff, which usually have time constants much longer than the response time of the system. In fact, this was verified in two patients in whom the regulation system was able to compensate for considerable cuff leaks that had been managed with difficulty in the conventional setting (fig. 3).

From a practical viewpoint, which is of crucial importance for routine clinical application, the main feature of the procedure described is its simplicity.

First, it is easily implemented because it does not require expensive or sophisticated instrumentation (fig. 1). As it does not require electronic circuitry, specialised technical or engineering personnel, the system can be implemented in the ICU. Second, it is simple to operate since *P*cuff is automatically and continuously regulated. Third, the procedure can be used to maintain *P*cuff regardless of the specific ventilator or endotracheal tube employed.

The combination of simplicity and effectiveness is the most distinct characteristic of this procedure, when compared with alternative methods previously proposed to control cuff inflation. Indeed, most of these devices are not automatic and/or need frequent control by the attending staff [17–19]. Moreover, other devices operating in a more automatic and continuous way are complex, require the use of special and expensive equipment [13, 20, 21] or require a special endotracheal tube (e.g. Lanz system; Mallincrodkt Medical) not available routinely. It is probable that these issues concerning complexity and cost could explain the lack of continuous automatic control of cuff inflation in clinical practice. The simple and cheap procedure the authors describe may facilitate the routine maintenance of adequate cuff inflation during mechanical ventilation.

The final step in the aetiopathogenesis of VAP is the aspiration of oropharyngeal secretions to the lower airways. The aspiration of pooled secretions between the endotracheal tube and the tracheal wall may be partly avoided using endotracheal tubes with a subglottic drainage aspiration lumen [22]. Continuous aspiration of subglottic secretions (CASS) may decrease or delay the incidence of VAP [23, 24]. However, CASS needs specific types of endotracheal tubes that may not be available at the time of intubation. Because the authors' devised procedure is potentially applicable in any clinical environment requiring intubation regardless of the specific type of ventilator or endotracheal tube used, it can be implemented at any time during the mechanical ventilation period without needing to replace the endotracheal tube, a risk factor for acquiring VAP [25]. In addition, CASS may be insufficient to prevent VAP when cuff inflation decreases, allowing pooled secretions to fall distally to the lower airways. Because cuff leaks are frequent in mechanically ventilated patients [10, 11], and loss of cuff inflation as a result of checking or maintaining pressure is a clear risk factor for VAP acquisition [11], maintaining the pressure of the cuff to avoid aspiration of pooled secretions is mandatory.

The authors' device would complement or substitute the use of subglottic aspiration tubes, and using this application alone or in combination with other simple measures, such as the semirecumbent position [26], could be useful in reducing the risk of ventilator-associated pneumonia. In addition, it would be cheaper compared to other strategies or even to the use of endotracheal tubes with subglottic drainage. Consequently, a randomised study to test the authors' technique in the prevention of ventilator-associated pneumonia is warranted.

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